INTRODUCTION

Root perforation is a pathologic communication between the root canal system and supporting tissues of the tooth through the root canal wall or the pulp chamber floor. The etiology of furcation perforation may be pathological (extensive caries, root resorption) or iatrogenic resulting from procedural accident during access preparation via an incorrectly directed bur, dealing with calcified pulp chambers or during post preparation (1, 2). The affected tissues respond through varied levels of inflammation, and the outcome of repairing root perforations depends on several factors such as the time elapsed before repairing the defect, location of the perforation, the adequacy of perforation seal and the size of the perforation (3).

Although several materials have been recommended for sealing root perforation, mineral trioxide aggregate (MTA) considered the gold standard and the material of choice (4, 5). The biocompatibility of MTA, its ability to seal root perforations effectively and its setting properties in the presence of moisture or even blood are important characteristics that may result in greater success rates when used for treating root perforations (4, 6, 7). Animal studies, case reports, and case series are available on the successful use of MTA as a perforation sealing material (8, 9). In vivo studies on furcation perforation revealed that MTA induced the formation of mineralized tissue (10, 11).
However, MTA is relatively expensive and hard to manipulate, especially in small defects. Researchers and clinicians have reported that it exhibits poor handling characteristics beside long setting time and tooth discoloration (4, 12). In a recent systematic review and meta-analysis, MTA appeared to enhance success rate up to 80.9% (13).

An artificial floor technique was introduced by Alhadainy et al. (14) for the repair of furcation perforation. In addition to control the extension of the repair materials, artificial floor excludes epithelial tissues from the sites of bone formation to help the regeneration of periodontal tissues. The artificial floor should be biodegradable material such as calcium sulphate that has been to act as a good barrier against the extrusion of the repair materials (1, 14).

A nano-filled resin modified glass ionomer (Nano-FRMGI) restorative material (glass ionomer that is modified by adding nano-sized resinous fillers) has been introduced for restoration of primary teeth and small cavities in permanent teeth. The Nano-FRMGI bonds effectively to enamel and dentin and its bonding mechanism could be attributed to micro-mechanical interlocking provided by the surface roughness, most likely combined with chemical interaction through its acrylic itaconic acid copolymers to get the best adhesion (15).

However, the problem with furcation perforation repair is still not agreed on as there is no currently available material meets all the ideal requirements of an ideal repair material as defined in the literature. Therefore, the objective of this study is to compare the tissue reaction of two repairing materials for furcation perforations (Nano-FRMGI and MTA) used with or without calcium sulphate artificial floor (CSAF).

**MATERIALS AND METHODS**

The protocol of this study was approved from the committee of dental research and ethics of institution in accordance with international agreements of World Medical Association Declaration of Helsinki “Ethical Principles for Medical Research Involving Human Subjects, October 2013” at (www.wma.net).

This study involved 96 teeth from 6 healthy adult male dogs, weighting between 11 to 17 kg and more than 1 year old. Each dog was numbered by a collar tag for consistent identification. Both sides of the mandibular and maxillary premolars, first and second molars were used (16 teeth per dog). The 96 teeth were divided into 4 groups (n=24) according to the furcation repair material. G1: MTA (Pro Root MTA, Dentsply Tulsa Dental, Tulsa, OK, USA), G2: MTA with CSAF (CAPSET, Lifecore Biomedical, Inc, Chaska, MN), G3: Nano-FRMGI (3M ESPE, Germany), G4: Nano-FRMGI with CSAF.

**Operative procedures**

Each dog was medicated with an intramuscular injection of acepromazine (Prom Ace S- AVECO, Fort Dodge, Iowa) at 0.2 mg/ kg dosage for sedation to allow its safe handling. At the same time, the dog received an intramuscular injection of atropine sulphate in a dose of 0.04 mg/kg to decrease salivary secretions. One dose of penicillin (Penicillin G Benzathine and Penicillin G Procaine) was also intramuscularly given at 30,000 U/Kg as prophylactic against infection. Each dog was placed under general anaesthetic by a veterinarian via intravenous injection of a mixture of ketamine hydrochloride and Xylazine in ratio of 1:2.

Preoperative radiographs were taken for all teeth before beginning of any operative procedures to confirm absence of periapical pathologies and complete root formation. A diamond bur (Mani Inc, Touchigi-Ken, Japan) in high-speed handpiece with water-cooling was used to reduce the cusps until until the pulps were exposed; coronal access openings were prepared with #2 round bur in a low-speed handpiece. After pulpectomy, the working length was determined 2 mm short of the radiographic apex. Instrumentation of the canal was completed with nickel-titanium K-files (Dentsply/Maillefer Corporation, Zurich, Switzerland) using a step-back technique and irrigation of root canals with 2.5% sodium hypochlorite were performed after each file. All prepared root canals were filled with gutta percha (Dentsply/Maillefer Corporation, Zurich, Switzerland) and AH26 sealer (Dentsply/Maillefer Corporation, Zurich, Switzerland) using cold lateral compaction technique.

A 1.4 mm diameter perforation was created in the center of the pulp chamber floor of the experimental teeth using a sterile #2 round bur (Dentsply/Maillefer Corporation, Zurich, Switzerland) at low speed. The perforation depth was limited to 2 mm into the alveolar bone. This was guided by using preoperative radiograph (parallel technique) and a rubber stopper as a marker on the shank of the bur. Sodium hypochlorite solution was used to irrigate the perforations and followed by normal saline solution. Bleeding was controlled and swabbed with sterile cotton pellets. Materials were prepared according to the manufacturers’ instructions and gently placed into the perforations. After setting of the materials, the coronal access cavity was sealed with light-cured composite resin (Filtek™ Z250 XT, 3M ESPE). Two dogs were sacrificed at each interval (1, 3, and 6 months) with a 150 mg/kg overdose of sodium pentobarbital (65 mg/mL) (Altabarak 10st Alkopa, Cairo, Egypt). Evaluation of the tissue reaction was made histologically.

**Histological evaluation:**

The teeth with surrounding bone were block sectioned and placed immediately in 10% neutral buffered formalin for tissue fixation and decalcified for 8 weeks using formic acid-sodium citrate. After dehydration and histological processing, Step-sessional sections of each block were cut using a microtome at a setting of 6µ thickness through the area of the furcal perforation in longitudinal sections parallel to the mesiodistal plane. Slides were stained with hematoxylin and eosin. Slides were then examined under light microscopy and photographs of selected areas were taken using a digital camera.

The histological sections were assessed for inflammation and type of healing at the furcation area adjacent to the repaired materials. The severity of inflammation was classified as in Table 1. The presence or absence of bone resorption, bone or cementum deposition, active of fibrosis, inflammation, regeneration PDL and epithelium at the furcation site were scored according to criteria used by AL Daafas and AL Nazhan (16).

**Statistical analysis**

Date were collected and tabulated, and descriptive statistics were presented as frequencies and corresponding percent-
Tissues responses for different treatment options and different time points:
Table 2 shows histological tissue reaction with different treatment options and different time points. Bone deposition was observed in up to 62.5% of cases in all groups. It occurred more frequently in MTA with CSAF and Nano-FRMGI with CSAF throughout the successive time intervals. However, bone resorption was found in 50% of cases after one month. In Nano-FRMGI, bone resorption decreased at 3- and 6-month observation. No single case of cementum deposition was reported in any group after one month. Afterward, cementum deposition increased gradually in MTA and MTA with CSAF at 3- and 6-month follow-up, while Nano-FRMGI and Nano-FRMGI with CSAF the increase was minimal.

Initial inflammation occurred in all groups with subsequent resolution of few cases through time except for Nano-FRMGI. Periodontal ligament (PDL) regeneration was observed in all groups through all time intervals, while MTA and MTA with CSAF were the highest percentage. Epithelium proliferation occurred in some cases of all groups after one month and disappeared with time in MTA and MTA with CSAF but oscillated in Nano-FRMGI and Nano-FRMGI with CSAF (Figs. 1-8).

Table 1. Classification of the severity of inflammation

<table>
<thead>
<tr>
<th>Scores</th>
<th>Classification</th>
<th>Description</th>
</tr>
</thead>
<tbody>
<tr>
<td>0</td>
<td>None</td>
<td>No infiltration of inflammatory cells</td>
</tr>
<tr>
<td>1</td>
<td>Mild</td>
<td>Few scattered inflammatory cells</td>
</tr>
<tr>
<td>2</td>
<td>Moderate</td>
<td>Inflammatory cells did not obscure the normal tissues</td>
</tr>
<tr>
<td>3</td>
<td>Severe</td>
<td>Massive infiltration of inflammatory cells replaced normal tissue</td>
</tr>
</tbody>
</table>

Inter-groups comparison, Chi square test showed no statistical significant difference between groups at any time interval (P > 0.05). However, intra-group comparison, mean rank test indicated a significant difference between 1-month interval and 6-month interval in cementum for MTA-alone (P < 0.05).
DISCUSSION

The material used in direct contact with living tissue should meet certain standards of tissue compatibility, in addition to any therapeutic or mechanical benefit that it may provide. Therefore, this study was conducted to investigate the tissue response to different repairing materials and techniques used in repairing furcation perforations and dogs appear to possess the most suitable model characteristic to furcation perforation studies (17).

Initial high inflammatory response was found with all groups at one-month interval that decreased gradually in the subsequent intervals. These finding are in accordance with other studies (14, 15).

Severity of inflammation for different treatment options and time intervals:

Table 3 represents the severity of inflammation induced by the used materials in all time points observations. All the materials used induced some degree of inflammation ranging from mild to moderate. Unlike Nano-FRMGI and Nano-FRMGI with CSAF, the inflammation resolved with time in MTA and MTA with Calcium sulfate.
ings agreed with previous findings (26-27) and may be related to the resin content of Nano-FRMGI which has been reported to liberate unbound substances from methacrylate derivative which has been shown to be not only a cytotoxic agent but also a genotoxic agent (24). In addition, substances leached from glass ionomer were also cytotoxic (25).

Bone apposition increased with time and bone resorption decreased for all materials except in Nano-FRMGI group. This agreed with the findings of (14, 16, 19-20). The use of CSAF increased bone deposition more than groups with repairing materials used alone. CSAF may accelerate the rate of mineralization of new bone by providing a source of calcium ions (28), prevent extrusion of repairing material into the peri-radicular space and its rate of resorption coincides with rate of bone growth that aids in tissue regeneration and excludes epithelium from the site of bone formation (29-30). These findings confirmed with previous studies (14, 31-34) that reported that the use of calcium sulphate under MTA provided the highest scores of bone deposition at 3-month evaluation period.

A high percentage of bone deposition in MTA with or without calcium sulphate at all intervals that increased with time is in accordance previous reports (16, 19, 29-30, 32-33) and (38). That can be explained by the favourable properties of MTA as mineral oxides content, non-cytotoxic, good biological compatibility and repair stimulation that allows cellular adhesion, growth and tissue proliferation on its surface (35-37).

Low percentage of bone deposition and inflammation in Nano-FRMGI at all time intervals compared with other groups agreed with previous studies (20, 26-27) and may be attributed to its initial good sealing ability which is followed by leakage due to seal breakdown by microbes from subgingival plaque.

Abscess was formed in one sample of Nano-FRMGI group at 3-month interval and another at 6-month interval. These findings agreed with previous findings (26-27) and may be related to the resin content of Nano-FRMGI which has been reported to liberate unbound substances from methacrylate derivative which has been shown to be not only a cytotoxic agent but also a genotoxic agent (24). In addition, substances leached from glass ionomer were also cytotoxic (25).

Bone apposition increased with time and bone resorption decreased for all materials except in Nano-FRMGI group. This agreed with the findings of (14, 16, 19-20). The use of CSAF increased bone deposition more than groups with repairing materials used alone. CSAF may accelerate the rate of mineralization of new bone by providing a source of calcium ions (28), prevent extrusion of repairing material into the peri-radicular space and its rate of resorption coincides with rate of bone growth that aids in tissue regeneration and excludes epithelium from the site of bone formation (29-30). These findings confirmed with previous studies (14, 31-34) that reported that the use of calcium sulphate under MTA provided the highest scores of bone deposition at 3-month evaluation period.

A high percentage of bone deposition in MTA with or without calcium sulphate at all intervals that increased with time is in accordance previous reports (16, 19, 29-30, 32-33) and (38). That can be explained by the favourable properties of MTA as mineral oxides content, non-cytotoxic, good biological compatibility and repair stimulation that allows cellular adhesion, growth and tissue proliferation on its surface (35-37).

Low percentage of bone deposition and inflammation in Nano-FRMGI at all time intervals compared with other groups agreed with previous studies (20, 26-27) and may be attributed to its initial good sealing ability which is followed by leakage due to seal breakdown by microbes from subgingival plaque.

Abscess was formed in one sample of Nano-FRMGI group at 3-month interval and another at 6-month interval. These findings agreed with previous findings (26-27) and may be related to the resin content of Nano-FRMGI which has been reported to liberate unbound substances from methacrylate derivative which has been shown to be not only a cytotoxic agent but also a genotoxic agent (24). In addition, substances leached from glass ionomer were also cytotoxic (25).

Bone apposition increased with time and bone resorption decreased for all materials except in Nano-FRMGI group. This agreed with the findings of (14, 16, 19-20). The use of CSAF increased bone deposition more than groups with repairing materials used alone. CSAF may accelerate the rate of mineralization of new bone by providing a source of calcium ions (28), prevent extrusion of repairing material into the peri-radicular space and its rate of resorption coincides with rate of bone growth that aids in tissue regeneration and excludes epithelium from the site of bone formation (29-30). These findings confirmed with previous studies (14, 31-34) that reported that the use of calcium sulphate under MTA provided the highest scores of bone deposition at 3-month evaluation period.

A high percentage of bone deposition in MTA with or without calcium sulphate at all intervals that increased with time is in accordance previous reports (16, 19, 29-30, 32-33) and (38). That can be explained by the favourable properties of MTA as mineral oxides content, non-cytotoxic, good biological compatibility and repair stimulation that allows cellular adhesion, growth and tissue proliferation on its surface (35-37).

Low percentage of bone deposition and inflammation in Nano-FRMGI at all time intervals compared with other groups agreed with previous studies (20, 26-27) and may be attributed to its initial good sealing ability which is followed by leakage due to seal breakdown by microbes from subgingival plaque.
There was decrease in bone resorption by time in MTA with or without calcium sulphate, while Nano-FRMGI group showed increased bone resorption over time. These findings were in agreement with Alhadainy et al. (14) who reported calcium sulphate with the lowest bone resorption that decreased with time when used to repair furcation perforation in dog’s teeth. The increased bone resorption in Nano-FRMGI agrees with Al-Hezaimi et al. (26). However, the initial bone resorption may be due to the low thermal trauma generated while perforating. Although low speed was used, increased temperature may have been generated when inserting the bur into the alveolar bone. This may have caused resorption and deposition of new bone and cementum.

Bone remodelling with new deposition was found more often in MTA with or without calcium sulphate. The bone deposition after resorption is called reversal lines which are scalloped rough lines. That represent the terminal of resorption process, new osteoblasts differentiated and deposited bone tissue. Thus, the resorption cavities were filled with new bone and bone surface was gradually smoothed in late process (16).

There was no increase in epithelial proliferation in MTA neither alone nor with calcium sulphate. While Nano-FRMGI had the highest epithelial proliferation at all intervals. The presence of epithelial proliferation in the perforation areas had been reported in previous studies (14, 16). MTA with or without calcium sulphate showed no epithelial tissue at 6-month interval. This may be due to its good biocompatibility and sealing ability (19). The epithelium detected probably resulted from the trauma that occurred during the perforation of the furcal area. The presence of epithelium may also be explained by the fact of the proximity of the dog’s teeth CEJ to the furcation area might be a limitation for using dog model studying the furcation perforation (40).

Periodontal ligament regeneration was observed in all groups through all time intervals, MTA alone or with calcium sulphate showed a higher percentage of PDL regeneration at all intervals. However, there was no statistical differences between groups at any time interval. This is referred to that MTA consistently allows the overgrowth of cementum and may facilitate the regeneration of the PDL and formation of bone. When used in dogs’ teeth with incomplete root formation and contaminated canals, MTA often induced the formation of apical barrier with hard tissue. The artificial floor maintained the MTA in situ may be interesting, permitting this material acting for more time. The effect of calcium sulphate is consistent with previously obtained results (14, 16, 29).

No cementum apposition was detected in any group at 1-month interval, but it was detected in all groups at 3- and 6-month intervals. MTA and MTA/CSAF had the same percentage that was higher than Nano-FRMGI and Nano-FRMGI/CSAF. These results support reports of perforation repair when using MTA (19, 29, 38, 41-43). Newly formed cementum may be derived from either the remaining PDL or ingrown connective tissue (42). This findings strongly support the role of calcite crystals and fibronectin as an initiating step in the formation of a hard tissue barrier (44). The calcite crystals were observed with reaction of calcium hydroxide content of MTA when contact the connective tissues (43).

**CONCLUSION**

In conclusion, within the limits of this study, it appears that Nano-FRMGI should not be the material of choice for repairing furcal perforations that accidentally occurs during endodontic treatment. Calcium sulphate under MTA provided the best results for repairing the accidental furcation perforation.
REFERENCES